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11-6

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# Quantitative contrast-enhanced ultrasound imaging of breast cancer

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## **Breast cancer**

#### Leading Sites of New Cancer Cases and Deaths 2022 Estimates



### Incidence:

no. 1 for cancer cases in women (31%)

### Mortality:

no. 2 for cancer deaths in women (15%)

	Female		
	Breast	287,850	31%
	Lung & bronchus	118,830	13%
7	Colon & rectum	70,340	8%
	Uterine corpus	65,950	7%
	Melanoma of the skin	42,600	5%
	Non-Hodgkin lymphoma	36,350	4%
	Thyroid	31,940	3%
	Pancreas	29,240	3%
	Kidney & renal pelvis	28,710	3%
	Leukemia	24,840	3%
	All sites	934,870	

Female

<u>Lung &amp; b</u> ronchus	61,360	21%
Breast	43,250	15%
Colon & rectum	24,180	8%
Pancreas	23,860	8%
Ovary	12,810	4%
Uterine corpus	12,550	4%
Liver & intrahepatic bile duct	10,100	4%
Leukemia	9,980	3%
Non-Hodgkin lymphoma	8,550	3%
Brain & other nervous system	7,570	3%
All sites	287,270	

# **Diagnostics and screening**



### Screening by mammography + lesion biopsy

12% suspicious of which 4% positive  $\rightarrow$  many unnecessary biopsies

### MRI advised for high-risk groups

### **Complemented by B-mode ultrasound**

<sup>1</sup> Zhi et al. Academic Radiology 2010
<sup>2</sup> Stanzani et al. Clinics 2014
<sup>3</sup> Wang et al. European Radiol 2016
<sup>4</sup> Zhao et al. OncoTargets and Therapy 2017
<sup>5</sup> Kapetas et al. Invest Radiol 2019

<sup>6</sup> Li et al. UMB 2020

### **Challenge: lesion classification**

- Elastography<sup>1</sup>
- Doppler<sup>2</sup>
- CEUS<sup>3,4</sup>
- Multiparametric<sup>5,6</sup>

# **Objective: CEUS imaging of breast cancer**

Rationale: cancer growth requires angiogenesis

Angiogenic microvasculature shows increased

- Density
- Tortuosity
- Irregularity
- Arteriovenous shunting



### Cancer angiogenesis

Folkman et al. *Nature*Brawer et al. *J Cell Biochem*Weidner et al. *Am J Pathology*Russo et al. *BJU Int*

# **CEUS features of breast cancer**

CEUS enhancement pattern	Malignant, n (%)	Benign, n (%)	χ²	Р
Distribution of contrast agent*			44.389	0.000
Homogeneous	3 (6.8)	46 (62.2)		
Heterogeneous	37 (84.1)	22 (29.7)		
Partial enhancement with perfusion defect	3 (6.8)	2 (2.7)		
Contour enhancement	1 (2.3)	4 (5.4)		
Enhancement time*			22.300	0.000
Earlier	39 (88.6)	34 (45.9)		
Synchronous	5 (11.4)	38 <b>(</b> 51.4)		
Later	0	2 (2.7)		
Enhanced intensity*			58.257	0.000
Hypo-enhancement	1 (2.2)	19 <b>(</b> 25.7)		
Iso-enhancement	5 (11.4)	44 (59.5)		
Hyper-enhancement	38 (86.4)	11 (14.9)		
Enhanced area enlargement*			67.266	0.000
None	2 (4.5)	61 (82.4)		
Yes	42 (95.5)	13 (17.6)		
Presence of radial or penetrating vessels*			58.092	0.000
None	6 (13.6)	63 (85.1)		
Yes	38 (86.4)	11 (14.9)		
Margin of enhanced lesion*			34.415	0.000
Clear	6 (13.6)	40 (54.1)		
Less clear	12 (27.3)	26 (35.1)		
Unclear	26 (59.1)	8 (10.8)		

### Heterogenous/irregular hyperenhancement

### → malignancy

Comparison of enhancement patterns between benign and malignant breast lesions.

Table 1

Enhancement patterns	Benign $(n=41)$	Malignant ( <i>n</i> = 86)	P value
Enhancement degree			< 0.001
Hypo-enhancement/iso-enhancement	33(80.5%)	32(37.2%)	
Hyper-enhancement	8(19.5%)	54(62.8%)	
Enhancement order			< 0.001
Centrifugal/diffused	31(75.6%)	26(30.2%)	
Centripetal	10(24.4%)	60(69.8%)	
Internal homogeneity			< 0.001
Homogeneous	29(70.7%)	22(25.6%)	
Heterogeneous	12(29.3%)	64(74.4%)	
Enhancement margin			< 0.001
Well defined	25(61.0%)	18(20.9%)	
Poorly defined	16(39.0%)	68(79.1%)	
Enhancement shape			0.021*
Regular	16(39.0%)	17(19.8%)	
Irregular	25(61.0%)	69(80.2%)	
Perfusion defects			< 0.001
Absent	36(87.8%)	45(52.3%)	
Present	5(12.2%)	41(47.7%)	
Surrounding vessels			< 0.001
Absent	33(80.5%)	33(38.4%)	
Present	8(19.5%)	53(61.6%)	
Diameter			0.003
Not enlarged	35(85.4%)	51(59.3%)	
Enlarged	6(14.6%)	35(40.7%)	

\*, statistical significance. CEUS, contrast-enhanced ultrasound.

Liu et al. Gland Surgery 2019

\* Enhancement shape (*P*=0.021) will not be significant after Bonferroni Correction.

#### Wang et al. European Radiol 2016

## 15 years of research on prostate cancer...



# **Contrast Ultrasound Dispersion Imaging** (CUDI)



### Cancer angiogenesis



Time intensity curves

### **Convective dispersion modeling**



 $\partial_t C = \nabla \cdot \mathbf{D} \nabla C - \vec{\nu} \cdot \nabla C$  $C(t) = \alpha \sqrt{\frac{\kappa}{2\pi t}} \exp\left(-\frac{\kappa}{2t} (t-\mu)^2\right)$ 

Dispersion map 🔶 Microvascular architecture

# **Contrast Ultrasound Dispersion Imaging** (CUDI)



### Cancer angiogenesis

### **Dispersion estimators**

Kuenen *et al. IEEE T-MI*Mischi *et al. IEEE T-UFFC*Kuenen *et al. IEEE UMB*Kuenen *et al. IEEE T-UFFC*Kuenen et al. *IEEE T-BME*Schalk et al. *IEEE T-UFFC*Schalk *et al. IEEE T-BME*van Sloun et al. *Med Im Analysis*van Sloun et al. *IEEE T-MI*Wildeboer et al. *IEEE T-MI*

### **Convective dispersion modeling**



 $\partial_t C = \nabla \cdot \mathbf{D} \nabla C - \vec{v} \cdot \nabla C$  $C(t) = \alpha \sqrt{\frac{\kappa}{2\pi t}} \exp\left(-\frac{\kappa}{2t} (t - \mu)^2\right)$ 

### Dispersion map 🚧 Microvascular architecture

# **Contrast Ultrasound Dispersion Imaging** (CUDI)







#### Dispersion maps



Histology









# **CUDI targeted biopsies**





Biopsies targeted by CUDI compared to systematic biopsy and mpMRI targeted biopsies in <u>142 patients</u>

Detection rates csPCa: SBx = 39% (56/142) mpMRI-TBx = 29% (41/142) CUDI-TBx = 28% (40/142)

Mannaerts et al. BJUI 2020

# 2D multiparametric ultrasound (mpUS)



Mannaerts et al. BMC Urology 2018

Mannaerts et al. J Urology 2019

Multiparametric ultrasound in the detection of prostate cancer: a systematic review

Arnoud Postema · Massimo Mischi · Jean de la Rosette · Hessel Wijkstra

World J Urol (2015) 33:1651-1659

1

GSU, C-TRUS, DCE-US and SWE are expected to show improved results in the near future. By effectively combining these ultrasound techniques, all targeting different properties of malignant tissue, a valuable clinical tool with all the advantages of ultrasound could be constructed. The literature shows that combining ultrasound modalities in a crude fashion can already improve sensitivity by 13–59 %.

DCE-US	Seitz et al. [33]	35	DCE-US versus RP and RCP	69	33	84	18
	Unpublished data from AMC	36	DCE-US + GSU versus RP	58–69	93–95		
	Unpublished data from AMC	11	Semiquantative DCE-US + GSU versus RP	87	84		
	Jung et al. [41]	20	Semiquantitative DCE-US versus RP	88	100		
SE	Zhang et al. [44]	508	Meta-analysis of 7 studies: SE versus RP	72	76		
	Teng et al. [45]	527	Meta-analysis: SE-targeted biopsy versus systematic biopsy	62	79		
SWE	Ahmad et al. [49]	50	Per ROI SWE versus 12 biopsies	90–93	88–93	93–98	83-81
	Barr et al. [48]	53	Per ROI SWE versus 12 biopsies	96	96	69	100

### **48 patients** B-Mode, CUDI, SWE



# Automatic zonal segmentation by deep learning





#### van Sloun et al. Eur Urol Focus 2019

# 2D multiparametric ultrasound (mpUS)





### Machine learning

(Random forest classifier)

# 48 patients

B-Mode, CUDI, SWE

Mannaerts et al. *BMC Urology* 2018 Mannaerts et al. *J Urology* 2019

Mode	de Parameter ROC-AUC per regi		Cper region
		≥3+3	>3+4
B-mode	G, gray level	0.53	0.58
SWE	E, Young's modulus	0.62	0.73
DCE-US	<i>v</i> , contrast velocity (mm/s)	0.69	0.76
	r, similarity dispersion(-)	0.69	0.76
	PT, time to peak (s)	0.63	0.68
	Multi-Radiomic <i>v</i>	0.71	0.84
RF-classifier	Multiparametric score	0.75	0.90

Wildeboer et al. Eur Radiol 2019



# **3D CUDI**



### Advantages

- Entire gland in one go
- Faster clinical workflow
- Complete kinetic modeling





Schalk et al. *IEEE T-UFFC* 2015; Schalk et al. *UMB* 2018 Wildeboer et al. *IEEE T-MI* 2018; Wildeboer et al. *UMB* 2019





### Vascular reconstruction by tractography



van Sloun et al. Nature Scientific Reports 2018

# **3D mpUS: prediction of biopsy outcome**



### 54 patients compared to 12-core SBx





### Features

- B-Mode LogiqE9 (RIC9-5 probe)
- CUDI LogiqE9 (0.3 Hz, MI = 0.1, 2.4 mL SonoVue)
- SWE Aixplorer (multiplane 3D reconstruction)

Chen et al. IEEE IUS 2021

# **3D mpUS: prediction of biopsy outcome**



### 54 patients compared to 12-core SBx





Features

- B-Mode
- CUDI
- SWE

Chen et al. *Euroson* 2022

Machine learning (Gradient boosting)

	ROC curve area*
CUDI	0.81 ± 0.12
SWE	0.66 ± 0.12
CUDI + SWE	0.85 ± 0.11

\*9-fold cross validation

## **Breast cancer data – 2D CEUS**





B-mode

CEUS

- 120 patients (18-82 years, average: 52 years)
- B-Mode + CEUS + biopsy
- October 2015 September 2016

### **CEUS** setting

- Siemens Acuson S3000
- Linear transducer (9L4HD)
- CPS at 4 MHz
- MI ≤ 0.07
- 4.8-mL bolus of SonoVue

# **Enhancement heterogeneity**



Benign breast lesion with low enhancement heterogeneity



Malignant breast lesion with high enhancement heterogeneity

# **CEUS enhancement grade**



Grade 1, Hyper-enhanced



Grade 2, Partly enhanced

### Quantitative enhancement grading

- Enhancement ratio\*
- Average enhancement\*

#### \*At peak enhancement



Grade 3, Poorly enhanced



Grade 4, Hypo-enhanced

# **CUDI spatiotemporal analysis of CEUS loops**

Similarity between time intensity curves (TICs)



1.5 cm imes 1.5 cm



# **CUDI spatiotemporal analysis of CEUS loops**

### Similarity between time intensity curves (TICs)

### Spectral coherence (ho)

Mischi et al. *IEEE TUFFC* 2012 Kuenen et al. *UMB* 2013

### **Correlation coefficient (***r***)**

Kuenen et al. IEEE TUFFC 2013

### Mutual information (I)

Schalk et al. IEEE TBME 2016

$$I = \sum_{c \in Q} \sum_{\boldsymbol{x} \in \boldsymbol{Q}} P_{\boldsymbol{X},C}(\boldsymbol{x},c) \log \left( \frac{P_{\boldsymbol{X},C}(\boldsymbol{x},c)}{P_C(c)P_{\boldsymbol{X}}(\boldsymbol{x})} \right)$$

### Conditional entropy (H)

$$H = -\sum_{c \in Q} \sum_{\mathbf{x} \in \mathbf{Q}} P_{\mathbf{X},C}(\mathbf{x},c) \log\left(\frac{P_{\mathbf{X},C}(\mathbf{x},c)}{P_{\mathbf{X}}(\mathbf{x})}\right)$$



### **Results -** Mutual Information





6-mm benign ductal hyperplasia in a 60-year-old woman





10-mm malignant invasive ductal carcinoma in a 43-year-old woman

## **Results** - pixel level classification

1.2

0.8

0.8

1

T



mation (1)							
benign n = 17 malignant n = 28	Statistics of parameter difference at the pixel level						
		Parameter	Benign	Malignant	p valu		
-		Correlation coefficient (r)	0.115 ± 0.077	0.088 ± 0.082	0.043		
-	Patients of	Spectral coherence ( $ ho$ )	0.478 ± 0.201	0.416 ± 0.222	0.127		
	grade 1 (45/120)	Mutual information $(I)$	0.547 ± 0.253	0.478 ± 0.201	<0.00		
1 1.2 mation (I) benign n = 23 malignant n = 41		Conditional entropy (H)	5. 263 ± 0.357	5.525 ± 0.315	<0.00		
		Correlation coefficient (r)	0.103 ± 0.076	0.085 ± 0.080	0.189		
	Grouped patients of	Spectral coherence ( $ ho$ )	0.441 ± 0.208	0.412 ± 0.216	0.362		
	grade 1 or 2 64/120	Mutual information $(I)$	0.473 ± 0.266	0.322 ± 0.252	0.002		
		Conditional entropy (H)	5.351 ± 0.359	5.543 ± 0.299	0.002		
-			± 0.359	± 0.299			

p value

< 0.001

< 0.001

### **Results** - Lesion classification



Table 3 Comparison of diagnostic performance of spatiotemporal parameters							
	Parameter	Sensitivity (95% CI)	Specificity (95% CI)	AUC	P value		
	Correlation coefficient $(r)$	89.3% (72.5 96.9)	64.7% (40.5 86.7)	0.743	0.010		
Lesions of grade 1	Spectral coherence ( $ ho$ )	67.9% (48.3 82.7)	82.3% (57.3 100)	0.724	0.015		
(45/120)	Mutual information (I)	85.7% (68.2 96.4)	94.4% (68.8 100)	0.893	<0.001		
	Conditional entropy (H)	78.6% (60.8 92.9)	88.2% (41.7 100)	0.874	<0.001		
	Correlation coefficient ( $r$ )	80.5% (66.7 90.5)	66.5% (37.8 75.0)	0.704	0.008		
Grouped lesions of grade 1 or 2	Spectral coherence ( $ ho$ )	63.4% (48.2 76.3)	75.9% (53.0 91.7)	0.670	0.034		
(64/120)	Mutual information (I)	90.2% (79.6 97.5)	82.6% (61.2 94.5)	0.848	<0.001		
	Conditional entropy (H)	78.1% (62.6 89.7)	78.3% (56.0 90.0)	0.817	<0.001		

# Conclusions

- CUDI spatiotemporal analysis of enhancing breast lesions (64/120) shows good classification performance, especially by mutual information (AUC=84.8%, Se=90.2%, Sp=82.6%)
- More quantitative parameters should be evaluated that reflect the complex perfusion patterns in breast lesions
- Hypoenhancing lesions call for a multiparametric approach involving other complementary features (texture, geometry, stiffness)

• 3D CEUS is expected to provide more accurate classification with motion compensation

# **Thank you!**

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11-6

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